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FUNCTIONAL INDICATORS OF PERIPHERAL ARTERIAL STIFFNESS IN SOLID ORGAN RECIPIENTS (LITERATURE REVIEW)

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Increased arterial stiffness is an important preclinical indicator of cardiovascular dysfunction, arterial hypertension and target organ injury. This condition increases the risk of long-term adverse events. Solid organ recipients face multiple risk factors for cardiovascular complications due to transplant rejection, lifelong medication use and adaptive features of the transplanted organ. The review presents an analysis of the results of studies on the main functional indicators of peripheral arterial stiffness, as well as the potential effect of immunosuppressive therapy on indicators of vascular stiffness in solid organ recipients.

Keywords: *stiffness, arterial stiffness, immunosuppression, recipients.*

Increased peripheral arterial stiffness is a biological process associated with increasing age [1, 2], blood pressure [3], inflammation [4, 5] and vascular calcification [6]. Arterial stiffness may also be related to donor age [7], arterial stiffness index in a related kidney donor [8], post-transplant diabetes mellitus [9], cold ischemia time [10], graft function [11], hypomagnesemia [12], and graft rejection [13]. In addition, immunosuppressive therapy may affect arterial stiffness or rigidity [14].

Arterial stiffness or rigidity has become virtually synonymous with pulse wave velocity (PWV), the rate at which pressure waves move down the vessel. Theoretically, this can be demonstrated in such a way that in an elastic tube of homogeneous structure with cross-sectional area A filled with a fluid of density ρ , a perturbation in the system propagates as a wave along this tube at the PWV and is expressed by the Bramwell–Hill equation (Bramwell J.C., Hill A.V., 1922):

$$PWV = \sqrt{\frac{A \partial P}{\rho \partial A}},$$

where ∂A is the change in lumen area in response to a change in pressure ∂P .

$D = \frac{\partial A}{A \partial P}$, where D represents tube extensibility (defined as the relative change in cross-sectional area in response to pressure). Hence, $PWV = \sqrt{\frac{1}{\rho D}}$. Thus, higher

vessel stiffness (lower D) results in higher PWV. Despite some limitations, PWV measurement has several advantages for clinical practice. When measured segment

by segment (e.g., in the aorta), PWV gives an average value of its stiffness. In clinical practice, PWV is most often calculated using the formula $PWV = \Delta L / \Delta T$, where ΔL is the distance between two measurement points and ΔT is the time it takes for arterial pulse to travel from the proximal to the distal measurement point [15]. The aorta is the main elastic vessel in the body, PWV in the aorta or in its segments probably represents the most informative parameter. The most widely used method for measuring aortic PWV is carotid-femoral PWV, the transit time of which is estimated from Doppler signals measured on the carotid and femoral arteries, which are relatively close to the aorta [15].

There are several measurement devices available, including commercially available systems such as Complior [16], Sphygmocor [17], Pulsepen [18] and others, as well as specially designed data acquisition systems (which, for example, have been used in population-based studies by Framingham [19] and Asklepios [20]). Ideally, measurements are performed simultaneously; sequential measurements together with ECG synchronization are the best alternative method. Any ultrasound machine with a vascular probe can also be used, provided the methodology is followed and appropriate software is available. Difficulties arise when estimating the carotid-femoral pathway length: the intra-arterial distance must be estimated from measurements at the body surface, and the pulse wave does not travel strictly straight along a single pathway from the carotid artery to the femoral artery measurement site.

Although there are a number of different ways to determine the distance, which makes it challenging to standardize measurements, PWV is now often calculated

by multiplying 0.8 by the distance between the common carotid artery and the common femoral artery measurement site [21]. Carotid-femoral PWV is considered the reference standard for clinical trials in Europe and the United States because of the availability of a large database of reference values obtained throughout Europe [22] and studies demonstrating the prognostic significance of this parameter [23–26].

PWV measurements should be evaluated according to patient age. The 2007 European Society of Cardiology Guidelines defined a fixed threshold value of 12 m/s to identify patients at high cardiovascular risk [27]. Later, expert consensus set this value at 10 m/s [21].

Another indicator reflecting arterial stiffness is the augmentation index. The augmentation index is based on pulse wave reflection and is a common measure of arterial stiffness. The augmentation index is defined as the ratio of the augmentation of systolic blood pressure to pulse pressure. To calculate it, it is necessary to determine the point of confluence of the direct and reflected waves (inflection point). According to some observations, this inflection point corresponds to the blood flow velocity peak and several algorithms have been developed for its identification [28–30].

Characteristic impedance is another arterial stiffness indicator. It relates absolute arterial pressure at a certain location to absolute blood flow velocity at the same location in the absence of reflected waves [31]. Characteristic impedance (Z_c) is related to PWV by the formula: $Z_c = CIIB \times \rho$. Since blood density is approximately equal to unity, these values are numerically almost identical when expressed in cm/sec or in dyn·s per cm³ [31]. It is virtually impossible to measure characteristic impedance by non-invasive methods because of the difficulty in excluding reflected wave effects and errors in non-invasive measurement of blood flow velocity and pressure.

OTHER ARTERIAL WALL ELASTIC PROPERTIES

1. Arterial distensibility – the change in relative diameter (or area) with increasing pressure. It is inversely related to the modulus of elasticity.
 $\Delta D / \Delta P \times D \text{ (mmHg}^{-1}\text{)}.$
2. Distensibility coefficient – the relative change in vascular cross-sectional area per unit pressure
 $DC = [\Delta A / A] / \Delta P = 2 \times \Delta d / d / \Delta P.$
3. Compliance – the absolute change in diameter (or area) at a given pressure and a given vascular length
 $\Delta D / \Delta P \text{ (cm/mmHg) or (cm}^2\text{/mmHg)}.$
4. Bulk modulus of elasticity – the pressure step required theoretically to increase volume by 100%
 $\Delta P / (\Delta V / V) \text{ (mm Hg)} = \Delta P / (\Delta D / D) \text{ (mmHg)},$
without changing length.
5. Elastic modulus – the pressure step required theoretically to stretch the diameter 100% from a resting state at a fixed vascular length
 $(\Delta P \times D / \Delta D) \text{ (mmHg)}.$

PERIPHERAL ARTERIAL STIFFNESS AND IMMUNOSUPPRESSIVE THERAPY

It is known that pathological processes in the vascular wall are triggered by dysregulation of matrix metalloproteinase activity. The effect of immunosuppressive drugs on the activity of matrix metalloproteinases has been reported. Results from a study by Korean authors that examined the effects of cyclosporine on human umbilical vein endothelial cells revealed that the immunosuppressive agent activates most matrix metalloproteinases in endothelial cells, with the exception of MMP-2 [32]. A British study on laboratory animals examined the effect of cyclosporine, tacrolimus and rapamycin on intimal hyperplasia, expression of fibrosis-associated genes and deposition of extracellular matrix proteins. In all groups, there was a significant inhibition of matrix metalloproteinase (MMP)-2, MMP-9, tissue inhibitor of metalloproteinases (TIMP)-1, transforming growth factor (TGF)-beta and collagen III expression ($P < 0.001$) after 14 days, but deposition of extracellular matrix deposits increased [33]. Bianchi et al. investigated how cyclosporine affected the expression of vascular endothelial growth factor (VEGF) and MMP-2 in rat myocardium. In contrast to the control group, cyclosporine-treated laboratory mice showed structural myocardial changes, including fibrosis and degeneration as well as a significant increase in both MMP-2 and VEGF [34].

In a Dutch study including a cohort of 330 kidney transplant patients, PWV was found to be a prognostic factor for cardiovascular events, outcomes and survival, irrespective of patient age. Patients with a PWV of 7.5 m/s or higher had worse survival than patients with a PWV <7.5 m/s [35]. In a 2011 prospective study including 512 renal transplant recipients, PWV, central augmentation pressure, and augmentation index were measured at the time of renal transplantation. The mean follow-up period was 5 years, PWV and augmentation pressure were included in a model based on clinical variables and laboratory data to predict cardiovascular events. The addition of PWV and augmentation pressure data resulted in a 15.9% update and reclassification of cardiovascular events. Moreover, patients with a PWV of 8.1 m/s or higher had worse cardiovascular survival compared to patients with a PWV <8.1 m/s [36].

A study by Norwegian authors including 1,022 renal transplant recipients showed that below a threshold of 12 m/s, each 1 m/s increase in PWV starting at 8 m/s was associated with a 36% increase in mortality risk [37]. The presented study results demonstrate that PWV is a strong predictor of cardiovascular events and death, independent of age and other clinical or laboratory variables. The results also validate the findings of other studies that have been conducted involving different patient populations [38–40].

Results from early studies on the effects of calcineurin inhibitors on large artery function were conflicting. In a prospective study, Zoungas et al. compared PWV before and after renal transplantation in 36 patients [41]. Twelve months after transplantation, PWV improved in all patients regardless of the use of cyclosporine or tacrolimus, although the decrease in augmentation index was greater in patients receiving tacrolimus ($8.0 \pm 16.5\%$ vs. $27.4 \pm 18.2\%$; $P = 0.01$). In a small study by Covic et al., it was demonstrated that cyclosporine dramatically reduced the augmentation index [42]. However, the study lacked a control group, and the decrease in augmentation index after cyclosporine administration was linked to shorter reflected wave time, which may lead to increased PWV in the long term.

In the same period, a parallel study (including 250 stable renal transplant recipients) showed that cyclosporine increased augmentation index and blood pressure to a significantly greater extent than tacrolimus [43]. In 2007, Strozecki et al. compared PWV in 76 patients receiving cyclosporine and 76 patients taking tacrolimus [44]. The two study groups were matched for key clinical characteristics (age, blood pressure, duration of hemodialysis, diabetes mellitus). Higher PWV were found in the cyclosporine group compared to the tacrolimus group (9.33 ± 2.10 versus 8.54 ± 1.35 , respectively; $P < 0.01$). In another study by the same authors using stepwise multiple regression analysis, it was observed that age, male sex, mean arterial pressure, cyclosporine (compared with tacrolimus), and fasting glucose levels were independently linked to higher PWV [45].

The effect of cyclosporine on arterial stiffness is probably due to increased vascular tone or impaired vasodilatory properties of nitric oxide. Given that cyclosporine administration is associated with higher PWV, switching to tacrolimus may reduce arterial stiffness. This hypothesis was tested in a small study where stable kidney recipients who had been taking cyclosporine for more than 10 years were converted to tacrolimus. PWV and ambulatory daily blood pressure monitoring (ABPM) were measured at baseline and 3 months after conversion, and no differences were found in either blood pressure or PWV, probably due to the short time interval after drug change [46]. All the studies cited suggest a possible negative effect of calcineurin inhibitors, especially cyclosporine, on PWV. In a randomized clinical trial, 17 of 27 patients were switched from cyclosporine to everolimus 6 months after kidney transplantation. PWV remained stable in the everolimus group (9.50 ± 1.92 vs. 9.13 ± 1.62 m/s, Δ PWV -0.37 ± 1.14 m/s), whereas it was elevated in the cyclosporine group (9.93 ± 1.94 vs. 10.8 ± 2.24 m/s, Δ PWV $+0.89 \pm 1.47$ m/s) [47].

In a study by Gungor et al., no benefit in PWV or augmentation index (Aix) was found in patients treated with mTOR inhibitors (at least 6 months – either sirolimus or everolimus) compared with treatment with

calcineurin inhibitors (cyclosporine or tacrolimus) [48]. In linear regression analysis, only classical risk factors (age, blood pressure, cholesterol level, and proteinuria) were found to be predictors of arterial stiffness. In a more recent randomized clinical trial, the effects of switching late from calcineurin inhibitors (tacrolimus) to mTOR inhibitors (everolimus) were examined. The findings demonstrated that left ventricular hypertrophy decreased in both groups. As secondary outcomes, changes in blood pressure (ABPM) and PWV were measured both before and after switching. The tacrolimus group (25 patients) and the everolimus group (31 patients) had median post-transplant durations of 1.7 and 1.3 years, respectively. Despite the fact that most patients receiving everolimus had dipper status, blood pressure in both groups was very well-controlled 24 months after randomization; 30% of those receiving tacrolimus were non-dippers, compared to 22% receiving everolimus. PWV at baseline, at 12 and at 24 months were within the normal range, with no significant differences between the two groups [49].

Another study evaluated PWV and blood pressure (ABPM) [50]. PWV was measured in 277, 223 and 184 patients after 12 and 24 months. Patients who switched to everolimus had a slight decrease in PWV (month 12: 0.24 m/s; month 24: 0.03 m/s), whereas patients taking cyclosporine showed a progressive increase in PWV (month 12: 0.11 m/s; month 24: 0.16 m/s); baseline values were within normal limits (mean 7.8 m/s for the everolimus group and 7.6 m/s for the cyclosporine group). Follow-up at 24 months confirmed the prognostic value of PWV, as the incidence of cardiovascular events in the entire cohort was low (2.8% in the everolimus group and 4.8% in the cyclosporine group). Since even small changes (0.4–0.5 m/s) usually occur over a long period of time, the follow-up period (at 24 months) was probably insufficient to detect any significant changes in PWV [51, 52]. Since patients with initially high PWV tend to have a more rapid increase in PWV [53], it is possible that switching to mTOR inhibitors may be beneficial in this patient cohort.

CONCLUSION

Stiffness or rigidity of the elastic and muscular-elastic arterial wall is a known independent predictor of adverse cardiovascular events [54–56]. Clinical practice has widely adopted noninvasive methods for examining systemic and local stiffness based on the measurement of PWV, augmentation index and other indicators [57, 58]. Published reports on mechanisms of regulation and the effect of immunosuppressive medications on vascular wall stiffness markers suggest that reducing arterial stiffness may be a therapeutic target for improving the quality of life in solid organ recipients [59–62].

The authors declare no conflict of interest.

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